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Mini Review

Radiographic Features of Lateralized Reverse Shoulder Arthroplasty in Osteoarthritis

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Abstract

The number of reverse shoulder arthroplasties (RSAs) has increased tremendously over the last twenty years, with a substantial change from Grammont design to lateralized devices, having the goal of reducing the risk of complications and improve clinical outcomes.

Radiographic criteria have been established to evaluate lateralization in RSA and to speculate on their biomechanical and functional effects.

Some biomechanical changes produced by glenoid and/or humeral lateralization are not completely understood and require additional exploratory research, investigating issues that have not previously been studied in-depth.

This manuscript aims to outline the most common radiographic features evaluating lateralized RSA based on the evidence from literature. This paper should help the surgeon in the postoperative evaluation of lateralized reverse prosthesis and improve the surgical technique for implant positioning and fixation.

Keywords: Reverse shoulder arthroplasty, Center of rotation, Offset, Glenoid lateralization, Humerus lateralization

Background

RSA is a worldwide treatment to manage pain and improve shoulder function in patients with advanced gleno-humeral osteoarthritis. The main efforts of researchers were directed to address glenoid replacement, using devices that would preserve glenoid bone stock and ensure prosthesis stability [1]. The modified Walch classification described different glenoid deformities in primary osteoarthritis [2], while Favard and Coll reported variable grades of superior glenoid erosion in patients with cuff tear arthropathy (CTA) [3]. The modern software using 3D computed tomography (CT) scan for preoperative planning, demonstrated that glenoid deformity in osteoarthritis is multiplanar, thus changing our view and approach to shoulder replacement [4,5].

Good to excellent clinical outcomes have been reported with RSA in both, primary osteoarthritis and CTA [6,7]

The original design of Grammont RSA has a joint center of rotation (CoR) located medial to the glenoid-bone-prosthesis interface [8] and a neck-shaft angle (NSA) at 155° allowing the humeral tray to cover <50% of the glenosphere. These biomechanical features have the effects of lowering the humerus and increase deltoid tension [9]. Lacking appropriate tension of the deltoid may cause instability of the implant, which represents the most fearsome issue of RSA.

Lateralizing the glenoid improves deltoid wrapping and increases joint reaction forces, which may lead to greater stability [10]. Risk factors for RSA instability include shortening of the humerus, abnormal glenoid medialization and deficiency of the soft tissues [11-15]. Scapular notching, i.e erosion of the scapular neck as result of the abutment of the humeral cup on the glenoid during adduction, is the most common long-term radiographic complication of medialized reverse implant [16].

The main modification of the Grammont design directed to reduce the risk of scapular notching was the lateralization of the CoR. This change can be performed at the level of the baseplate, with bone or metallic increased offset implants (bony-increased offset RSA [BIO-RSA] and metallic-increased offset RSA [MIO-RSA]), or at the level of the glenosphere, changing its design. Lateralization of the CoR away from the glenosphere/glenoid interface increases the risk of mechanical loosening [17]. Changes of NSA, from 155° to 135°, and the new position of the reverse tray in onlay configuration, have produced a novel stem geometry that preserve the tuberosities, and the insertion of the rotator cuff (RC) (if present), with potential effects on external rotation recovery [18].

Radiographic Assessment of Lateralized RSA and Biomechanical Considerations

Radiographs to assess components position and lateralization of an RSA include true anterior-posterior (AP) Grashey, outlet and axillary views (**Figures 1A-1C**). Glenoid lateral offset (LO) is the sum of the radius of the glenosphere and of the CoR offset, and increases with increased glenosphere size. However, increasing the size of the glenosphere to the next available size, increases glenoid lateralization by a mean of only 1.14 mm. This is a very limited increase in lateral offset relative to CoR lateralization or humeral lateralization [19]. Therefore, glenoid lateralization is often referred to as CoR lateralization.







Figure 1. Standard radiograph series to assess the shoulder joint. A. True AP view, B. outlet view, C. axillary view. AP: Anterior-Posterior.

LO in RSA changed significantly, from the original medialized prosthesis of Grammont (mean 13.1 mm) to modern lateralized design (up to 35.8 mm).

Overall, the lateralization of the CoR can be achieved by either glenosphere shape modification or baseplate lateralization. When the RSA is medialized, compressive and shear components of the resultant force vector, act through a fixed CoR [8]. A CoR lateralization obtained through a specific glenosphere design, decreases compressive forces and increases destabilizing shear forces, creating a new moment (M) at the glenoid-implant interface [20] (Figures 2A-2B). When glenoid lateralization is achieved through the baseplate, the CoR falls at the interface baseplate-glenosphere. This design may theoretically reduce the micromotion at the glenoid bone-implant interface, and features that enhance fixation, such as larger screws, more screws, and porous coatings, can also contribute to minimize the risk of loosening. However, biomechanical studies supporting these speculations have not yet been published.

Preoperative CT planning guide the appropriate direction and orientation of glenoid baseplate and allows a perfect component seating (**Figures 3A-3C**).

BIO-RSA is a type of "biologic lateralization" based on the concept that increasing the length of the scapular neck would lateralize both, CoR and glenoid-implant interface [21]. This

would maintain the CoR at the glenoid-implant interface minimizing the torque on the glenoid component.

Radiographic evaluation of BIO-RSA includes assessment of bone graft radiolucency and thickness (mm) (**Figure 4**). Radiolucent lines >2 mm indicate that the bone graft is not healed and the baseplate is "at risk" of loosening. Glenoid radiolucent lines assessed at the interface "glenoid bone-metal" of MIO-RSA explain the baseplate seating (no radiolucent lines: perfect seating; radiolucent lines <2 mm: incomplete seating; radiolucent lines >2 mm: loosening).

Additional radiographic features around the glenoid component include: radiolucent lines (RL) (5 zones), scapular notching, formation of bone scapular spurs and ossifications [22]. Multiple RL <2 mm or one RL \geq 2 mm represent risk factors of glenoid loosening.

AP view radiographs are used to determine the vertical position of glenosphere according to the inferior glenoid rim (glenosphere inferior overhang [GIO]: high, flush, low and very low) [23] and glenosphere inclination, as measured by the β angle (global glenoid inclination) [24] and RSA angle [25] (**Figures 5A and 5B**). Insufficient GIO, following a high or flush placement of the glenospfere and a superior inclination of the baseplate (RSA >5°), are associated with higher risk of scapular notching. The best glenoid implant alignment should include a baseplate within 10° of neutral version in the axial plane and

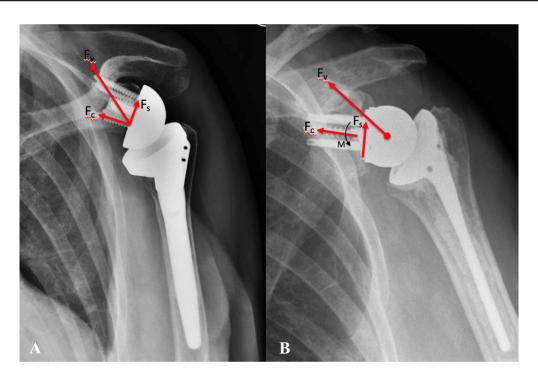


Figure 2. A. Reverse shoulder arthroplasty (RSA) acting with a fixed CoR with compressive (Fc) and shear (Fs) components of the resultant force vector (Fv). **B.** CoR lateralization increases the lever arm length which decreases compressive forces, increases destabilizing shear forces, and creates a new moment (M) at the glenoid-implant interface [34]. RSA: Reverse Shoulder Arthroplasty; CoR: Center of Rotation.





Figure 3. Preoperative planning of primary shoulder osteoarthritis: **A.** computed tomography scan showing increased glenoid retroversion and superior inclination (posterior-superior glenoid bone loss). **B.** posterior-superior augmented baseplate ("bone preserving baseplate") placed with a perfect seating (100% implant contact), - 6.5° inferior inclination and neutral glenoid version. **C.** Postoperative AP radiograph of the planned RSA with medium augmented baseplate and low GIO. GIO: Glenosphere Inferior Overhang; AP: Anterior-Posterior.

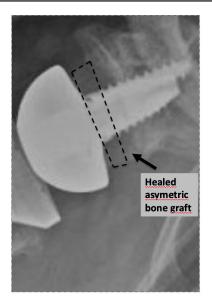
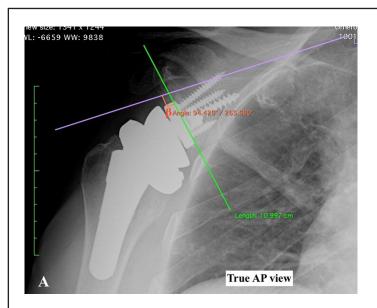


Figure 4. BIO-RSA with a healed bone graft (dotted line). The CoR remains at the glenoid-implant interface. BIO-RSA: Bone Increased Offset-Reverse Shoulder Arthroplasty; CoR: Center of Rotation.



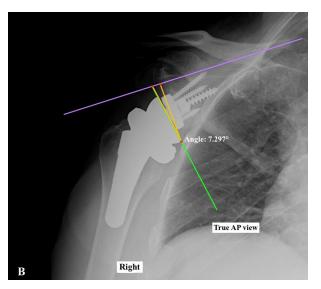


Figure 5. Angle beta is the angle between the floor of the supraspinatus fossa and the glenoid fossa line **(A)**. The RSA angle is the angle between the inferior part of the glenoid fossa (where the baseplate is implanted) and the perpendicular to the floor of the supraspinatus fossa **(B)**.

perpendicular to the floor of the supraspinatus fossa. The RSA angle and the β angle measure the focal inferior inclination and are helpful to determine the size of the bone or metallic augments needed to compensate for superior inclination in RSA [25].

Acromio-humeral distance and lateral humeral offset represent the amount of humeral distalization and lateralization and affect deltoid tension.

Additional radiographic methods described to measure

the inferior and lateral position of the humerus, include the distalization shoulder angle (DSA) and lateralization shoulder angle (LSA) [26] (**Figures 6A and 6B**).

Active range of motion after RSA is correlated with specific ranges of LSA and DSA. LSA between 75° and 95° is correlated with an increased active external rotation and a DSA between 40° and 65° is correlated with increased active anterior elevation [26].

Lateralization of RSA can be represented schematically as





Figure 6. Distalization shoulder angle (DSA) (A) and lateralization shoulder angle (LSA) (B).

described in the **Figure 7** [19]. Overall, lateralization in RSA can be performed on the glenoid side, humeral side or both (global lateralization).

Global lateralization is the sum of humeral LO and glenoid LO. The range of global lateralization that is possible to obtain with one given RSA implant varies from 3.3 to 20.9 mm [19]. Current RSA devices allow glenoid lateralization up to 7.7 with standard baseplate and up to 8.8 mm with bone or metallic augments.

Surgeon should be cautious with glenoid lateralization beyond +5–10 mm, depending on the amount of loss of medial bone stock, to avoid the risk of scapular facture or brachial plexus nerve palsy [10].

There is substantial evidence from biomechanical studies, that RSA design has effects on muscle moment arms [27]. The deltoid abductor moment arm increases with a medialized glenoid/lateralized humerus (MGLH) significantly more than lateralized glenoid/medialized humerus (LGMH) [27]. Improved deltoid efficiency has been documented by a reduction in

force to achieve humeral elevation. When the CoR is distalized, the lines of action of the subscapularis and infraspinatus are affected in such a way that these muscles induce a much larger adduction. Offset of the humerus affects the efficiency of posterior deltoid, while a lateral CoR did not affect muscle moment arm of external rotators [27]. These biomechanical findings confirm the efficacy of reverse design to improve deltoid lever arm when the CoR is located at the glenoid bone interface. The role of augmented glenoid component with specific design of baseplate, remains crucial to preserve glenoid bone stock in arthritic shoulders with severe glenoid erosion [28]. By using CT-based computer modeling, Slowinski and Coll found that an augmented baseplate preserved, on average, 54% more native bone than a nonaugmented baseplate and results in 4.1 mm of lateralization[28]. Correction for glenoid bone defects without removing excess healthy bone, may may prevent possible complications of impingement and scapular notching.

Despite the above reported biomechanical findings of Hamilton and co-workers [27] did not show significant effects of lateralized design on external rotators muscles, recent

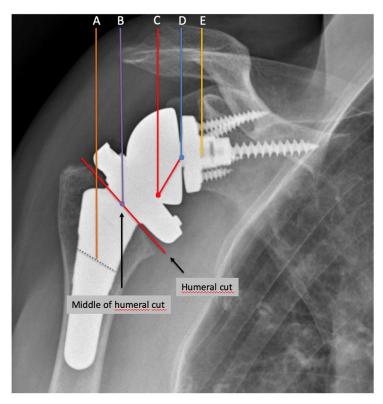


Figure 7. Radiographic references to measure humeral and glenoid offset in lateralized RSA (global lateral offset), as described by Werthel et al. [19]. Line A is the vertical line passing through the middle of the diaphysis of the humeral stem. Line B is the horizontal line passing through the middle of the surface of the humeral implant at the level of the humeral cut. Line C is the vertical line passing through the "pivot point" defined as the deepest point of the articular surface of the humeral insert measured perpendicular to the surface of the humeral insert. Line D is the vertical line passing through the centre of rotation of the joint. Line E is the vertical line passing through the bone-glenoid baseplate interface. Humeral lateral offset (distance AC) was defined as the sum of the humeral stem offset (distance AB) and of the humeral insert offset (distance BC). Glenoid lateral offset (distance CE) was defined as the sum of the "perceived radius of the glenosphere" (distance CD) and of the centre of rotation offset (distance DE).

clinical studies demonstrated that RSA with 135° NSA and a lateralized glenosphere enables better preservation of external rotation and reduces the rate of scapular notching compared with the classic Grammont design in patients with cuff tear arthropathy [29]. Similar clinical findings were reported in other research studies describing reverse design with humeral and glenoid lateralization [18,30,31]. The use of reverse design with lateralized CoR or global lateralization, have reduced the risk of scapular notching, almost eliminating it [18,31], but have increased the risk of scapular spine and acromial fractures [18,32] (**Figure 8**). The effects of lateralized RSA on internal rotation mobility are unclear and results of recent clinical studies, assessing different reverse design, are elusive.

Recent research findings showed that a larger glenosphere size, a posterior offset humeral cup and an increased inferior glenosphere overhang were associated with excellent outcomes [33].

Analysis of other established radiographic parameters (radiolucency, condensation lines, cortical thinning, spot

weld, subsidence and resorption of the tuberosities) complete the evaluation of the stemmed humeral component and give information about the stability of the humeral component and the risk of stress shielding and reduction of cortical thickness of the humerus [18].

Overall, lateralization in RSA can be performed on the glenoid side, humeral side or both (global lateralization).

Take Home message

Radiographic features described in this study represent a pictorial essay to assess lateralized RSA.

RSA with CoR lateralization, both with bone or metal, represents a strategic choice for glenoid replacement in cases with severe bone loss. The role of augmented glenoid component with specific design of baseplate, remains crucial to preserve glenoid bone stock in arthritic shoulders with severe glenoid erosion. Glenoid lateralization should instead be cautiously considered in patient with shoulder arthritis without severe glenoid deformity.

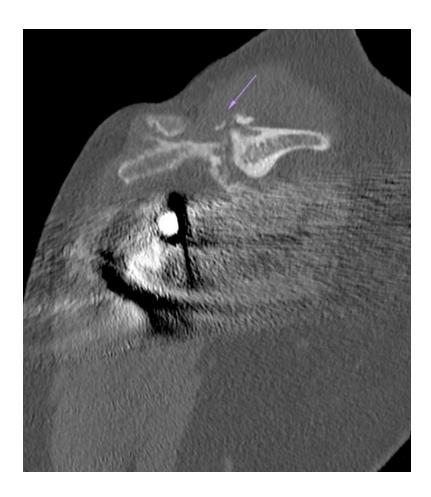


Figure 8. Scapular spine fracture (purple arrow) in lateralized RSA ("global lateralization").

Humeral lateralization improves posterior deltoid tension, while its action on the residual posterior rotator cuff muscles is still debated.

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Competing Interests

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